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## Correlation of Clinical Neuromusculoskeletal and Central Somatosensory Performance: Variability in Controls and Patients with Severe and Mild Focal Hand Dystonia

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### SUMMARY

Focal hand dystonia (FHD) is a recalcitrant, disabling movement disorder, characterized by involuntary co-contractions of agonists and antagonists, that can develop in patients who overuse or misuse their hands. The aim of this study was to document clinical neuromusculoskeletal performance and somatosensory responses (magnetoencephalography) in healthy controls and in FHD subjects with *mild* versus *severe* hand dystonia. The performance of healthy subjects ( $n = 17$ ) was significantly better than that of FHD subjects ( $n = 17$ ) on all clinical parameters. Those with *mild dystonia* ( $n = 10$ ) demonstrated better musculoskeletal skills, task-specific motor performance, and sensory discrimination, but the performance of sensory and fine motor tasks was slower than that of patients with *severe dystonia*. In terms of somatosensory evoked field responses (SEFs), FHD subjects demonstrated a significant difference in the location of the hand representation on the x and y axes, lower amplitude of SEFs integrated across latency,

and a higher ratio of mean SEF amplitude to latency than the controls. Bilaterally, those with FHD (*mild* and *severe*) lacked progressive sequencing of the digits from inferior to superior. On the affected digits, subjects with *severe dystonia* had a significantly higher ratio of SEF amplitude to latency and a significantly smaller mean volume of the cortical hand representation than those with *mild dystonia*. Severity of dystonia positively correlated with the ratio of SEF mean amplitude to latency (0.9029 affected, 0.8477 unaffected;  $p < 0.01$ ). The results of the present study strengthen the evidence that patients with FHD demonstrate signs of somatosensory degradation of the hand that correlates with clinical sensorimotor dysfunction, with characteristics of the de-differentiation varying by the severity of hand dystonia. If these findings represent aberrant learning, then effective rehabilitation must incorporate the principles of neuroplasticity. Training must be individualized to each patient to rebalance the sensorimotor feedback loop and to restore normal fine motor control.

### KEYWORDS

somatosensory evoked potentials, neuroplasticity, focal hand dystonia, magnetoencephalography

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## INTRODUCTION

Most tasks performed with the hands require delicate, complex, individuated, fine motor movements (Gerloff et al., 1996; Johansson, 1996; Sherrington, 1906). The hand has a large, orderly, somatotopic, highly differentiated representation in the sensory and motor areas of the brain (Iwamura et al., 1983; Iwamura et al., 1992; Jenkins et al., 1988; Kass et al., 1986; Penfield, 1950; Yang et al., 1994). These topographical representations are complemented by functional representations of well-learned tasks (e.g. writing) (Rijntjes et al., 1999).

Somatotopic and functional representations are modified by injury, development, learning, environmental enrichment, deprivation, disease, and practice. Representational changes can be modified over a lifetime by attended, goal-directed, rewarded, nonstereotypic, progressive spaced practice (Jenkins et al., 1990; Wang et al., 1994). Selective changes in cell assemblies can be driven by behaviors that selectively specialize hand representations in parallel with the emergence of more efficient, accurate, and differentiated behaviors. This neural adaptation has been extensively documented in terms of modulation in neural transmitters, myelination, synaptic and dendritic complexity, as well as function in studies involving animals (Allard et al., 1991; Hebb, 1949; Jenkins et al., 1990; Jenkins et al., 1990; Kass et al., 1983; Merzenich et al., 1983 a-b, 1984, 1991; Nudo et al., 1996 a-b, 1999, 2000; Penfield, 1950; Recanzone et al., 1992a-c; Wang et al., 1994, 1995; Yang et al., 1994; Zerri et al., 1996; 1999) and humans (Merzenich et al., 1996 a-c, 1998; Elbert et al., 1998; Nagarajan et al., 1997; Sanger & Merzenich, 2000; Spengler et al., 1997; Wright et al., 1997).

Despite the infinite degrees of freedom and permutations of a wide variety of movements, much of what we do becomes repetitive, stereotypic,

and automatic. Given the limits of neural adaptation, stressful, attended, stereotypic, near-coincident, repetitions can have negative consequences on motor performance, e.g. focal hand dystonia (FHD) (Bara-Jimenez et al., 2000; Byl et al., 1996 a-b; 2000 a-b; Chen et al., 1998; Mc Kenzie et al., 2000).

Focal hand dystonia, also referred to as occupational hand cramps, is one type of focal limb dystonia (Altenmueller, 1997). Involuntary co-contractions of agonists and antagonists cause writhing and twisting movements of the hand and wrist that interfere with controlled, target specific voluntary fine motor movements (Altenmueller et al., 1997; Bell, 1883; Cohen & Hallet, 1988; Cole et al., 1995; Fry, 1986; Hochberg et al., 1990; Jankovic & Shale, 1989; Marsden et al., 1990; Newark et al., 1987; Rothwell et al., 1983; Tubiana, 1983; Utti et al., 1995). Etiologic factors for focal dystonia range from genetics (Gasser et al., 1996; Illarioshkin et al., 1988; Leube et al., 1996; Ozelius et al., 1997), imbalance between the inhibitory and excitatory pathways in the globus pallidus (Black et al., 1998; DeLong et al., 1985, 1990; Perlmutter et al., 1997), cortical dysfunction (Chase et al., 1988; Defendini & Fahn, 1988; Deuschl et al., 1995; Gilman et al., 1988; Tempel, 1993; Toro, 2000), degradation of the somatotopic maps in the thalamus (Lenz et al., 1996; Utti, 1995), disruption of reciprocal inhibition at the level of the spinal cord, (Chen et al., 1995; Kaji et al., 1995; Nakashima et al., 1989; Naumann et al., 1997; Panizza et al., 1989, 1990), to secondary problems related to chronic pain, trauma, nerve root irritation, peripheral nerve entrapment, or anatomic restrictions (Charness et al., 1992; 1993; Katz et al., 1990; Leijinse, 1996; Quartarone et al., 1998; Topp & Byl, 1999; Wilson et al., 1991; 1993).

Initial evidence from animal and human studies implies that FHD could be a consequence of aberrant learning. Repetitive, near simultaneous, alternating, reciprocal digital movements, performed under stressful conditions, can lead to de-differentiation of the somatosensory hand representation that

disrupts sensory discrimination, sensorimotor feed back, and fine motor control (sensorimotor learning hypothesis) (Bara-Jimenez et al., 1998; Byl et al., 1996 a-c; 1997; 2000 a-c; Ikeda et al., 1999; Odergren et al., 1996; Sanger & Merzenich, 2000; Sanger et al., 2001; Tinassi et al., 1999). In one nonhuman primate model designed to test the sensorimotor learning hypothesis, owl monkeys performed attended, repetitive hand opening and closing (1.5 h/d) until they were unable to perform the task in a controlled way (simulating a target specific clinical hand dystonia) (Byl et al., 1996 c; 1997). Electrophysiological mapping revealed shrinkage of the somatosensory hand representation on the trained side, unusually large overlapping receptive fields bilaterally, and persistence of the same digital representations across broad columnar distances on the cortex bilaterally (Blake et al., 2002; Byl et al., 1996; 1997). Two of the primates did not work intensely and used the whole arm and the trunk rather than the hand alone to close the hand piece. These two monkeys did not develop a disorder in fine motor control (Byl et al., 1997). Magnetoencephalography studies of human subjects with FHD revealed similar somatosensory degradation (Bara-Jimenez et al., 1998; Chen & Hallet, 1998; McKenzie et al., 2000). The authors reported abnormalities in the area of the somatosensory hand representation on the trained side (e.g., reduction of in the spread of the digits and the overall hand area on the affected compared with the unaffected side) and the sequential ordering of the digits (e.g., loss of sequential digital ordering from inferior to superior bilaterally).

No intervention strategy has been one-hundred percent effective for restoring normal motor control in all FHD patients. Although botulinum toxin injections or baclophen can decrease dystonic cramping (Brin et al., 1987; Ceballos-Baumann et al., 1995; Cole et al., 1995; Fahn et al., 1987; Karp et al., 1994; Pullman et al., 1996; Tsui et al., 1993;

Van Hilten et al., 2000), the medications do not improve somatosensory differentiation and rarely enable musicians to return to their previous high levels of performance. Conservative intervention strategies based on the principles of neuroplasticity, including constraint induced therapy (Candia et al., 1999), sensitivity training (Tubiana et al., 1998), kinematic training (Mai et al., 1994), conditioning techniques (Liversedge et al., 1955, 1960), immobilization (Priori et al., 2001), and comprehensive sensory discrimination training (Byl et al., 2000 c) are being explored as alternate intervention strategies.

Although all FHD patients complain of uncontrolled, involuntary movements, primarily when performing a specific task, the clinical presentation varies from patient to patient. For example, certain patients have trouble in performing a single target task and others have difficulty with a variety of tasks, including uncontrolled movements with the involved digits simply with contact of the glabrous palm or digits with any surface. Some patients complain of a "dullness or numbness", whereas others complain of "increased sensitivity or jumpiness" of the dystonic digits. Possibly such clinical differences are related to the underlying somatosensory degradation. If this variability in response were more clearly understood, then intervention and prevention strategies could be tailored to the individual and potentially be more effective. The present study contributes to this gap in understanding.

We hypothesized that if FHD represented a learned de-differentiation of the cortical somatosensory organization of the hand, then clinical problems in sensory processing and motor control should be measurable. We also hypothesized that variations in clinical performance and somatosensory evoked responses should differentiate between subjects with *severe* versus *mild* hand dystonia.

## EXPERIMENTAL

### Subjects

The subjects were recruited from the Peter Ostwald Health Program for Performing Artists and the Physical Therapy Faculty Practice at the University of California, San Francisco (UCSF). Male and female subjects between 20 and 60 years of age were eligible to participate in the study. Each subject (1) had been diagnosed with a unilateral focal hand dystonia (FHD) based on an evaluation by a neurologist; (2) had demonstrated observable involuntary twisting movements of the digits and wrist when performing the target or similar tasks; (3) had normal reflexes and no evidence of a peripheral neuropathy or central nervous system pathology; (4) had a history of FHD for more than 6 mo; (5) worked in an occupation demanding repetitive use of the hands (e.g., computer use, card dealing, playing a musical instrument, writing, court reporting); and (6) had not received an injected or systemic drug to control the dystonia for more than 6 mo before admission to the study.

The subjects lived in the San Francisco Bay area or were willing to stay there for several days to complete the testing. From a previous database of healthy controls, two groups of healthy subjects were age and sex matched and then randomly selected as historic reference controls. The purpose and procedures of the study were explained to each subject, and signed consent was obtained before testing. The study was approved by the UCSF Committee on Human Research.

### Procedures

A broad battery of standardized clinical tests were administered to each FHD subject ( $n = 17$ ) and to all historic controls ( $n = 17$ ). The test procedures and the reliability of testing described

in prior studies are summarized in Table 1 (Byl et al., 1996 a-b; 2000 a-c; 2002). Specific subtests were summed into seven dependent variables:

1. physical musculoskeletal performance (selected range of motion, strength, neural tension);
2. sensory discrimination (graphesthesia, localization, kinesthesia, stereognosis)
3. fine motor efficiency (Purdue Test-time), fine motor skill (line tracing accuracy and time) and digital reaction time (averaged across the 5 digits for each hand);
4. motor control at the target task;
5. posture and balance;
6. functional independence; and
7. pain.

The subtests allowed for the comprehensive measurement of clinical performance. By combining the scores into seven dependent variables, we could control for the experiment-wise error in the study. Low intercorrelations between each summated dependent variable ( $r < 0.1$ ) suggested that the dependent variables were measuring a unique characteristic (Byl et al., 2000 a). All subjects with FHD were classified as having simple (dystonia limited to one target task) or dystonic dystonia (dystonic movements occurred with the target task, tasks similar to the target task, or surface contact of the hand). All subjects with FHD were first rated in terms of severity according to the Tubiana Dystonia Scale for Musicians (Tubiana et al., 1998):

- 0 = unable to do the target task;
- 1 = able to do limited aspects of the task or perform the task for very short periods;
- 2 = able to do the task with modification of technique;
- 3 = able to do the task but not efficiently or with normal quality).

Then, for purposes of correlational analysis, all subjects with FHD were classified into one of two

**TABLE 1**  
Summary of Clinical Test Procedures

Measurement Tool	Dependent Variable	Scoring System	Directions	Reliability	Equipment
<b>Graphesthesia</b> (Modified Subtest of Sensory Integration Praxis Test [SIPT])	Sensory Performance	2=correct, 1=partially correct, 0= incorrect; % error calculated.	Tip of a paperclip used to draw designs on subject's fingers while eyes closed (EC). Subject recreates design with pen with eyes open (EO). 2 designs per finger pad.	Interrater= 0.95, Test-retest r= 0.91. (Ayres, 1989; Mailloux et al, 1991)	Paper-clip and design sheet.
<b>Kinesthesia</b> (Subtest of SIPT)	Sensory Performance	Average error (distance from target) in mm.	Subject's hand is moved to target and back to start position; subject attempts to relocate digit, EC. 5 trials per hand.	Interrater= 0.95 Test-retest r= 0.90. (Mailloux, et al 1990; Mulligan, 1992; Byl et al, 1996)	Target sheet and ruler.
<b>Byl-Cheney-Boczar Test (BCB) for Stereognosis</b> (Byl et al., 2002)	Sensory Performance	2=correct, 1=partially correct, 0= incorrect; % error calculated.	Subject's finger is drawn across the shape twice, EC. Subject attempts to pick correct shape. 10 trials for 2 <sup>nd</sup> and 4 <sup>th</sup> finger pads.	Interrater/ intrarater =0.995 (ICC), correlation of r=.60 b/w BCB and Purdue Test (Byl et al, 2000c; Lafayette Instruments <sup>1</sup> )	20 designs and test sheet of designs
<b>Digital Reaction Time</b>	Fine Motor Performance	Time in msec, average of all trials.	Subject turns stopwatch on/off as quickly as possible. 3 trials per finger.	Intrasession reliability ranges from 0.975-0.99 (Bohannon, 1995)	Stopwatch.
<b>Purdue Test</b>	Fine Motor Performance	Total time to put pegs in and out.	Subject puts 25 pegs into a board and then removes.	0.60-0.63. (Lafayette Instruments)	Watch, peg-board.
<b>Manual Muscle Test</b>	Musculo-skeletal Performance	Kilograms of force: UE and LE Scores total all scores. <sup>2</sup>	Performed per procedures defined by Kendall (Kendall and McCreary, 1983) with dynamometers added to increase objectivity used for grip, key and pinch grip.	R=0.887 multiple correlation with MMT	Jamar Microfet and Baseline dynamometers

<sup>1</sup> Lafayette Instrument Company, PO Box 5729 Lafayette IN 47903, (317 423-1505)

<sup>2</sup> Muscle groups tested: hip flexors and extensors, knee flexors and extensors, ankle dorsiflexors, elbow flexors, shoulder flexors, wrist extensors, lumbricals, grip and pinch (3-jaw chuck and key grip) strength.

**TABLE 1**  
Summary of Clinical Test Procedures

Measurement Tool	Dependent Variable	Scoring System	Directions	Reliability	Equipment
<b>Range of Motion</b>	Musculo-skeletal Performance	Degrees; sum of active and passive.	Performed measurement procedures defined by Norkin (Norkin and Levangie, 1992). Arm, wrist and hand joints summed to a upper extremity score and joints in the leg summed lower extremity score and then totaled.	Intratester: $r=0.91-0.99$ .	Goniometer
<b>Posture and Balance</b>	Postures and balance	Ordinal scales; coded 2 if fully met the criteria, 1 if partially met the criteria and 0 if did not meet the criteria	Posture: bony landmarks cited for the line of gravity (Kendall and McCreary, 1983) were coded as 0-2 and summed to a total. Balance score summed from: Feet together, (eyes open and eyes closed for 20 seconds), one foot (eyes open and eyes closed for 10 seconds) and tandem romberg (eyes open and eyes closed for 10 sec.)		
<b>CAFÉ 40</b>	Functional Performance	7 point Likert Scale (1=least independent 7=most independent).	Self-scoring of ability to perform functional activities. Scores inverted for data analysis.	Test-Retest: $r=0.971$ . (Fung et al, 1997)	Written questionnaire.

categories: *mild or severe*. Those with simple dystonia rated as 0 or 1 were classified as *severe dystonia* and those rated 2 or 3 as *mild dystonia*. All subjects with dystonic dystonia were rated as 0 or 1 and classified as *severe dystonia*.

Somatosensory testing was carried out according to standard protocols by trained research assistants. All testing in the Biomagnetic Imaging Laboratory at UCSF was performed by trained staff (Roberts et al., 1998; Rowley et al., 1995). The test-retest values for the magnetic source imaging testing established in this lab are high ( $> 0.9$ ) (Spengler et al., 1997). A 37-channel biomagnetometer (Magnes II, 4D Neuroimaging, 1.5 fT, San Diego, California) placed in a magnetically shielded room with two circular sensors (14.4 cm) was used to create a magnetic source image of the hand. Two hundred and fifty air puffs were delivered within 1 cm<sup>2</sup> sacs, for 30 msec, at 17 to 20 pounds psi, with a pseudorandom interstimulus interval 450 to 500 msec. The stimulus served as a super-threshold force designed to indent the skin 400 microns. Each digit was stimulated on the distal pad, middle and proximal segment on each digit on each hand. In addition, a similar stimulus was delivered to each side of the upper lip. Preliminary studies demonstrated that a psi of 15 was adequate to evoke a somatosensory field response, and that the latency and amplitude of this response were not significantly enhanced by a stimulus of 20 or 25 psi for normal subjects or for subjects with dystonia (See Fig. 1).

A normal somatosensory-evoked field response (SEF) elicited by the pneumatic cutaneous response is characterized by a peak amplitude at a latency between 30 and 70 msec, subject to a signal to noise ratio greater than 4, goodness of fit (model/data)  $> 0.95$ , with a minimal confidence volume less than 3000 mm<sup>3</sup> (Roberts, et al., 1998; Rowley et al., 1995). The dependent variables, recorded for each SEF response, included latency (msec), root mean square (rms) amplitude across sensor channels

(fT), and location of the digits on the x, y, and z axes (cm). The following variables were determined: (1) amplitude of the SEF was integrated over time; (2) ratio of mean SEF amplitude to latency was calculated; (3) order of the digits on the z axis, plotted inferior to superior from D1 to D5; (4) spread of digits, calculated by subtracting the maximum centimeter distance between the most widely separated digits; and (5) volume of the digital representation, calculated based on the formula for an ellipsoid ( $4/3 \pi$  times the radius of the spread on x, y, and z axes).

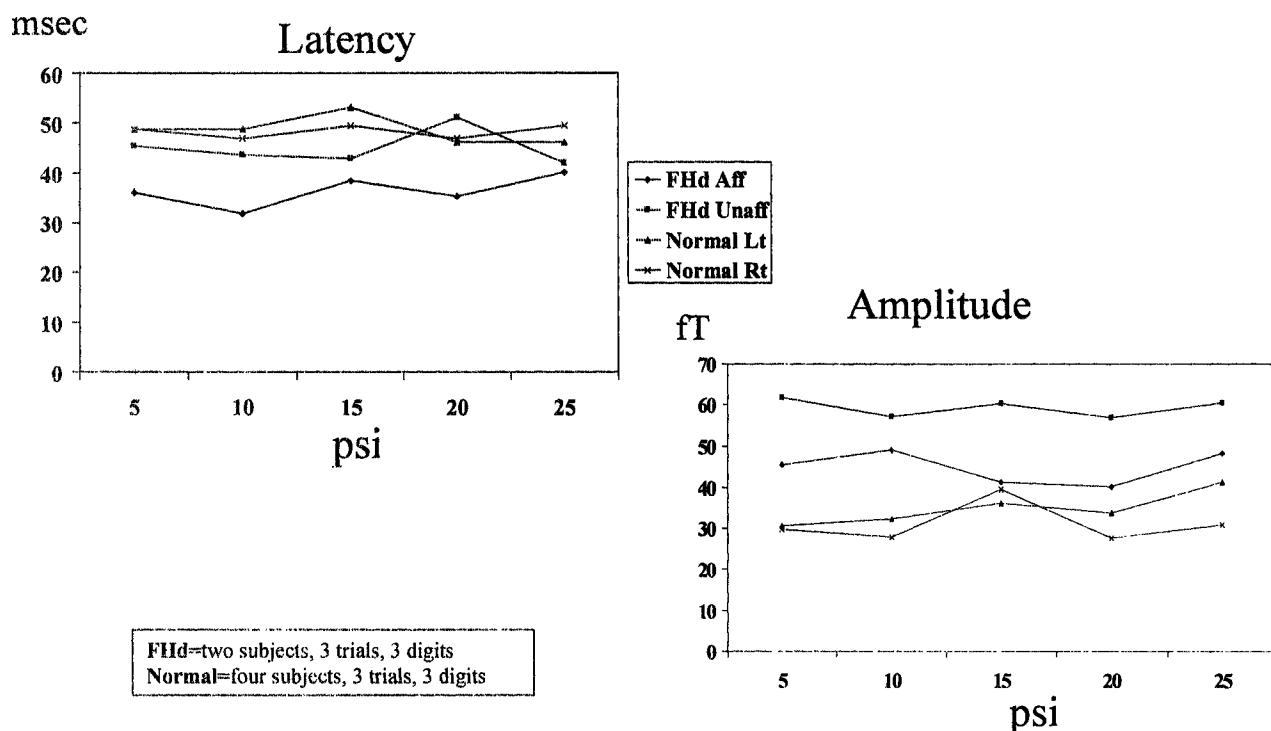
### Research design

This was a descriptive study including three groups of subjects. All dependent variables were described by mean and standard deviation (SD). Line graphs and scatter plots were created for visual analysis of the relation of SEF amplitude across latency. Given the low correlation between the dependent variables, each dependent variable for each limb was considered independent. Thus, we tested each dependent variable for significance at  $p \leq 0.05$  (two-tailed). Where multiple subtests were combined or multiple trials were combined to create a dependent variable, the number of measurements was based on the number of subjects times the number of test components/ trials.

### Data analysis

Based on the somatosensory and clinical dependent variables, we analyzed the differences between controls and FHd subjects and within subjects with FHd using the Student *t* test or an analysis of variance (ANOVA) for the dependent variables measured with ratio data or the Wilcoxon Ranked Sum or Wilcoxon Two-Sample Test for the dependent variables measured on an ordinal scale. The severity groupings for the FHd subjects were correlated with clinical performance parameters and





**Fig. 1:** Latency and amplitude of somatosensory evoked field response (SEF) by stimulus force. Controls and subjects with mild versus severe FHd. There were no consistent differences in the latency or the amplitude of the somatosensory evoked response between 5 and 20 psi for the healthy control subjects (4 subjects, 3 trials, 3 digits) or those with focal hand dystonia (2 subjects, 3 trials, 3 digits). The amplitude did increase slightly when the stimulus force was increased to 25 psi.

somatosensory variables, with *mild dystonia* coded as 1 and *severe hand dystonia* coded as 2 in the correlation matrices. The correlations were tested for significance using the Z-test for Correlation Coefficients based on preliminary studies, with an effect size of 1.0, alpha at .05 and beta at .20, a total of 15 subjects was needed to achieve a power of 80% for finding a significant difference.

## RESULTS

There were 9 males and 8 females with FHd between the ages of 23 and 55 years [with a mean of  $39.9 \pm 11.1$  years]. All worked in jobs requiring

repetitive hand movements. Ten were musicians. Eleven of the FHd subjects had simple dystonia and six had dystonic dystonia. Ten subjects could no longer practically perform the task and were classified with *severe dysonia* and seven could perform the task for short periods of time with modification of technique and were classified with *mild dystonia* (Table 2). The 15 subjects in the control group for somatosensory measurements ranged in age from 23 to 57 years with a mean age of 37.4 years ( $\pm 9.7$  years). There were 8 males and 7 females. Two were musicians and the other subjects worked in jobs requiring repetitive hand use on a computer keyboard (Table 3). Of the 17 reference controls selected for comparing clinical

**TABLE 2**  
Description of subjects with focal hand dystonia

Age	Gender	Hand Dominance	Occupation	Type of Dystonia <sup>1</sup>	Severity <sup>2</sup>	Involved Side/Digits	Wrist Flex/Ext
22	F	R	Musician flute	Simple	1	L3-5	No
26	M	R	Musician bagpipe	Simple	2	L3-5	No
28	M	R	Musician- guitar	Simple	1	R2	No
29	F	R	Computer Programmer	Simple	0	L1-5	No
36	M	R	Card Dealer	Simple	2	R1-2	No
30	F	R	Musician- violin	Simple	2	L2-5	No
41	M	R	Physician	Dystonic	1	R1-2	Yes
37	F	R	Musician- flute	Simple	1	L4-5	No
50	M	R	Musician- saxophone	Dystonic	0	L1-5 R1-5*	Yes
50	F	R	Word Processing-Computer	Dystonic	0	L1-5	Yes
44	M	R	Administrator-High computer use	Simple	2	R1-3	Yes
52	M	R	Pianist-Band Leader	Simple	2	R2-5	Yes
35	F	R	Pianist-composer	Simple	2	R1-5	Yes
45	M	L	Musician-oboe	Simple	2	L3-5	No
44	M	R	Guitarist-Programmer	Dystonic	1	R1-5	No
45	F	L	Musician-piano	Dystonic	1	R1-5	Yes
65	F	R	Word Processor	Dystonic	1	R4-5	No

The focal hand dystonia subjects comprised 9 males and 8 females between the ages of 23 and 55 years (mean 39.9 years). Eleven of the FHd subjects were classified as having simple dystonia and six with dystonic dystonia. Ten were classified as having severe dystonia (rated 0-1 on the Tubiana Scale). Ten were musicians , one (\*) previously diagnosed with FHd on the opposite side.

**<sup>1</sup>Type of Dystonia:**

Simple: movement dysfunction only on one target task

Dystonic: movement dysfunction on a variety of similar tasks

**<sup>2</sup>Severity of target specific dystonia:**

0 unable to do the target task;

1 able to do limited aspects of the task or perform the task for very short periods;

2 able to do the task with modification of technique;

3 able to do the task but not efficiently or with normal quality (105)

**TABLE 3**  
Description of healthy control subjects

Age	Gender	Hand Dominance	Repetitive hand use	Occupation
22	F	R	High level of computer use and manual therapy	Graduate Student
28	M	R	High level of computer use and manual therapy	Graduate Student
28	M	R	High level of computer use and manual therapy	Graduate Student
28	F	R	High levels of computer use –Data analysis	Graduate Student
32	M	R	High levels of computer use-Data analysis	PhD Researcher
35	F	R	High repetitive hand use on Musical instrument	Musician
38	M	R	High level of computer use-data analysis	PhD Researcher
40	F	R	High levels of computer use-data analysis	Post Doc Researcher
50	M	R	High levels of computer use	Administrator
50	F	R	High repetitive hand use on musical instrument	Musician
30	M	R	High levels of writing	Graduate student
30	F	R	High levels of writing	Graduate student
50	M	R	High level of computer use-data analysis	Research Scientist
42	M	R	High levels of computer use	Business administrator
58	F	R	High level of computer use	Educator

The control group comprised 7 females and 8 males between the ages of 22 and 58 years (mean age 37.4 years). All healthy control subjects were involved in jobs demanding high levels of repetition; two were musicians.

performance, there were 5 males and 12 females with an average age of 30.2 years ( $\pm 3.6$  years). The majority of control subjects who volunteered for the clinical measurements were graduate students, faculty, or friends of students or faculty who had a history of repetitive hand use (e.g. intensive note taking and computer use).

Table 4 summarizes the results of the clinical performance parameters for patients with FHd and healthy controls. Compared with healthy controls, patients with FHd performed significantly worse when using either the affected or unaffected side in terms of musculoskeletal skills, fine motor control, and sensory discrimination. Scores for posture and

**TABLE 4**Clinical performance of controls and FHd subjects by severity of dystonia<sup>1, 2, 3</sup>

Dependent Variables	No. subtests	Range	Affected Side FHd		Unaffected Side FHd			
			Severe n = 10	Mild n = 7	Severe n = 10	Mild n = 7	Right	Left
Physical performance	4	30-350	235.9 (36.6) *7	261.0 (35.8) *7	273.7 (32.5)	275.7 (42.3)	295.1 *1 (25.1)	289.4 *2 (24.2)
Balance/Posture	2	0-100	87.1 (12.2)	90.9 (4.5)	87.1 (12.2)	90.9 (4.5)	96.6 (3.6)	
Fine Motor Skills	6	70-450	189.4 (34.4)	198.1 (5.2)	186.7 (48.2)	191.4 (42.3)	139.0 *3 (25.5)	139.0 *4 (25.6)
Task Specific Motor Control	1	0-100	49.0 (12.7) *8	59.5 (5.4) *8	89.5 (8.0) *9	64.6 (9.9) *9	NA	
Sensory Skills	6	30-380	276.3 (67.0) +	274.8 (12.9) +	211.8 (65.9)	231.8 (66.1)	175.0 *5 (29.6)	172.1 *6 (16.5)
Independence	2	0-100	91.7 (5.98)	93.5 (4.8)	91.7 (5.98)	93.5 (4.8)	91.9 (5.6)	
Pain	2	0-100	88.7 (9.5)	96.4 (5.0)	99.0 (3.2)	100.0 (0)	97.2 (6.8)	97.4 (6.1)

The clinical tests were summed to measure seven clinical dependent variables. The clinical performance scores were significantly lower for FHd subjects compared with control subjects. Compared with those with severe focal hand dystonia, FHd subjects with mild dystonia demonstrated better physical performance, were slower but more accurate in sensory and fine motor performance, and demonstrated bilateral problems with task specific motor control.

<sup>1</sup> FHd (n=17) Controls (n=17)

<sup>2</sup> Differences between Controls and FHd Subjects (combined across groups):

<sup>3</sup> Differences between those with mild and severe dystonia

**Critical Values:**

\*1, t= 4.6 (p<0.001);

\*4, t= 13.6 (p<0.001);

\*7 t=4.50; p<0.001;

\*2, t=3.12 (p<0.002)

\*5, t= 8.66 (p<0.001)

\*8 t=3.09; p<0.01;

\*3; t= 6.09 (p<0.001);\*

\*6, t=8.87; (p<0.001);

\*9 t=8.00; p<0.0001

+ Although the total sensory score was not significantly different, there was a significant difference in the subtests in terms of time for sensory processing (87.4 (53.8) for those with severe dystonia compared with 125.2 (68.9) for those with mild dystonia (t=2.04; p<0.05) and accuracy 50.4 (26.1) for those with severe dystonia compared with 26.1 (27.0) for those with mild dystonia (t=2.22; p<0.05).

**Definitions:**

Severe Dystonia: included Dystonic Dystonia (0-3) Simple (0-1)

Mild Dystonia: Simple Dystonia- 2-3

**Scale Scores:**

Physical performance, balance/posture, independence, pain = high scores are good

Motor skills and sensory skills = low scores are good

balance were lower for FHd subjects than controls, but the differences were not significant. There were no differences between the groups in terms of pain or functional independence. On the affected limb, those with *severe dystonia* had reduced performance measurements in musculoskeletal skills and target specific motor control compared with those with *mild dystonia*. Although the overall sensory discrimination accuracy was low for all FHd subjects (with no significant differences by severity), for tasks that included speed and accuracy, those with *severe dystonia* performed the tasks faster than those with *mild*

*dystonia*. On the *unaffected* side, those with *mild dystonia* demonstrated greater inaccuracy when performing the target specific task.

There were no significant differences between mean SEF latency or mean SEF amplitude for FHd subjects and reference controls, but the location of the digits on the x (bilateral) and y axes (affected) were significantly different ( $p < 0.0001$ , respectively) and the ratio of SEF mean amplitude to latency was higher for FHd subjects compared with the controls ( $p \leq 0.05$ ). On the unaffected side, the volume of the hand representation was significantly larger for FHd subjects than for controls ( $p < 0.05$ ) (see Table 5).

TABLE 5

Differences in somatosensory responses for controls and subjects with FHd<sup>1</sup>

	Affected Side		Unaffected Side	
	Controls	Subjects	Controls	Subjects
Latency (msec)	45.9 (7.4)	43.6 (4.0)	45.1 (7.8)	44.1 (4.3)
Amplitude (Ft)	45.2 (20.6)	54.4 (12.1)	48.7 (18.8)	46.7 (7.4)
Ratio (Amplitude to Latency)	1.08 (0.6) *4	1.36 (0.7)*4	1.20 (0.6)	1.31 (0.8)
Location (cm)				
Axis x	1.25 (0.3)*1	1.7 (0.3)*1	1.21 (0.2)*2	2.00 (0.4)*2
Axis y	3.84 (0.5)*3	4.3 (0.3)*3	3.95 (0.3)	3.90 (0.2)
Axis z	9.32 (0.3)	9.5 (0.9)	9.58 (0.3)	9.50 (0.4)
Spread (cm)				
Axis x	0.63 (0.2)	1.0 (0.4)	0.60 (0.3)	0.84 (0.4)
Axis y	1.04 (0.4)	1.3 (0.8)	0.91 (0.5)	1.07 (0.5)
Axis z	0.94 (0.4)	1.1 (0.4)	0.89 (0.3)	1.10 (0.5)
Volume (cm <sup>3</sup> )	0.39 (0.2)	0.58 (0.5)	0.26 (0.3)*5	0.67 (0.6)*5

As measured by magnetoencephalography, there were no significant differences in the mean amplitude and latency of the somatosensory evoked field responses for controls and those with FHd. However, compared with controls, the FHd subjects had a higher ratio of the mean amplitude to mean latency on the affected side, there was a significant difference in location of the digits on the x and y axes, and the area of the hand representation was significantly greater on the unaffected side.

<sup>1</sup>Controls: n=15; Subjects: n = 17

\*significant  $t_1=7.62$ ;  $p < 0.0001$ ;  $t_2=7.60$ ;  $p < 0.0001$ ;  $t_3=5.93$ ;  $p < 0.0001$ ;  $t_4=2.05$ ;  $p < 0.05$ ;  $t_5=2.12$ ;  $p < 0.05$

TABLE 6

Somatosensory evoked field response by severity of dystonia: digit spread by axes and volume

Spread of digits	Affected Side		Unaffected Side	
	Controls	Subjects	Controls	Subjects
Axis x	1.05 (0.61)	0.82 (0.31)	1.18 (0.56)	0.822 (0.30)
Axis y	1.32 (0.67)	1.01 (0.52)	1.08 (0.57)	0.761 (0.32)
Axis z	0.81 (0.98)	0.90 (0.42)	1.11 (0.41)	0.782 (0.52)
Volume (cm <sup>3</sup> )	0.71 (0.69) *1	0.45 (0.38) *1	0.82 (0.76) *2	0.524 (0.52) *2

\*1  $t=2.15$  ( $<0.05$ ); \*2  $t=2.00$  ( $<0.05$ )

On both the affected and unaffected side, the volume of the representation of the hand was significantly larger for those with mild compared with those with severe hand dystonia.

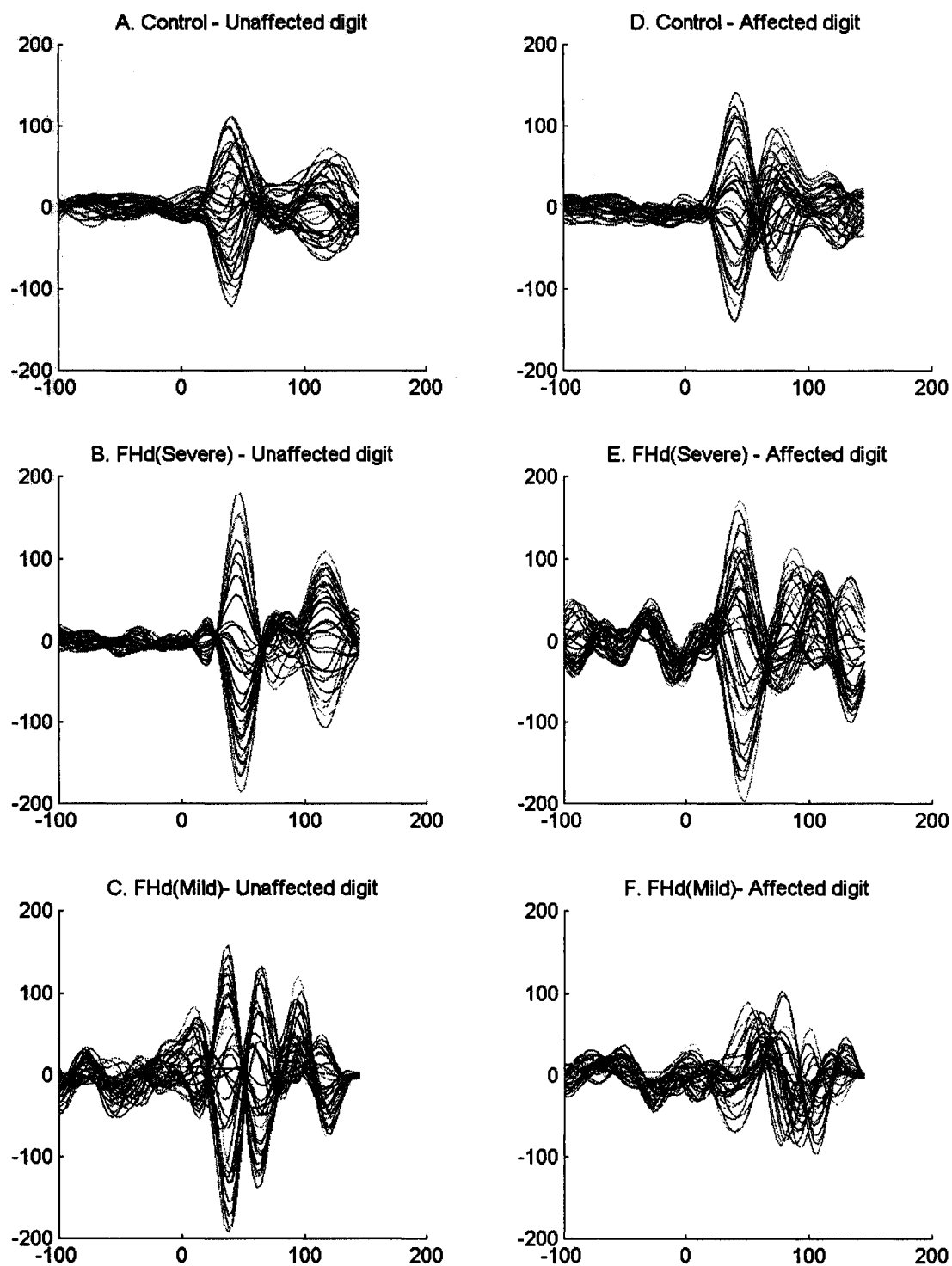
Table 6 summarizes the parameters of the somatosensory evoked field responses (SEFs) for those with *mild* versus *severe dystonia*. Bilaterally, for those with *mild dystonia*, the volume of the representation of the hand was significantly larger than in those with *severe dystonia*.

Figure 2 illustrates the different patterns of the somatosensory evoked field responses (SEFs) for the digits for one control and two subjects with FHD. The patterns of the SEFs for controls and those with FHD were similar on the lip (uninvolved body part), but the SEF patterns for the digits were different for healthy controls when compared with those of subjects with FHD. The pattern of the SEF for the control subject (A and D) was characterized with a primary burst of activity at 40 msec at an amplitude between 70 and 100 fT, quieting at 120 msec. For the subject with *severe dystonia* (B and E) on both sides, the first burst of activity was  $<40$  msec with an amplitude of  $> 150$  fT and either a second burst of activity or continued activity (60 fT) after 120 msec. On the unaffected side for the subject with *mild dystonia*, the SEF(C)

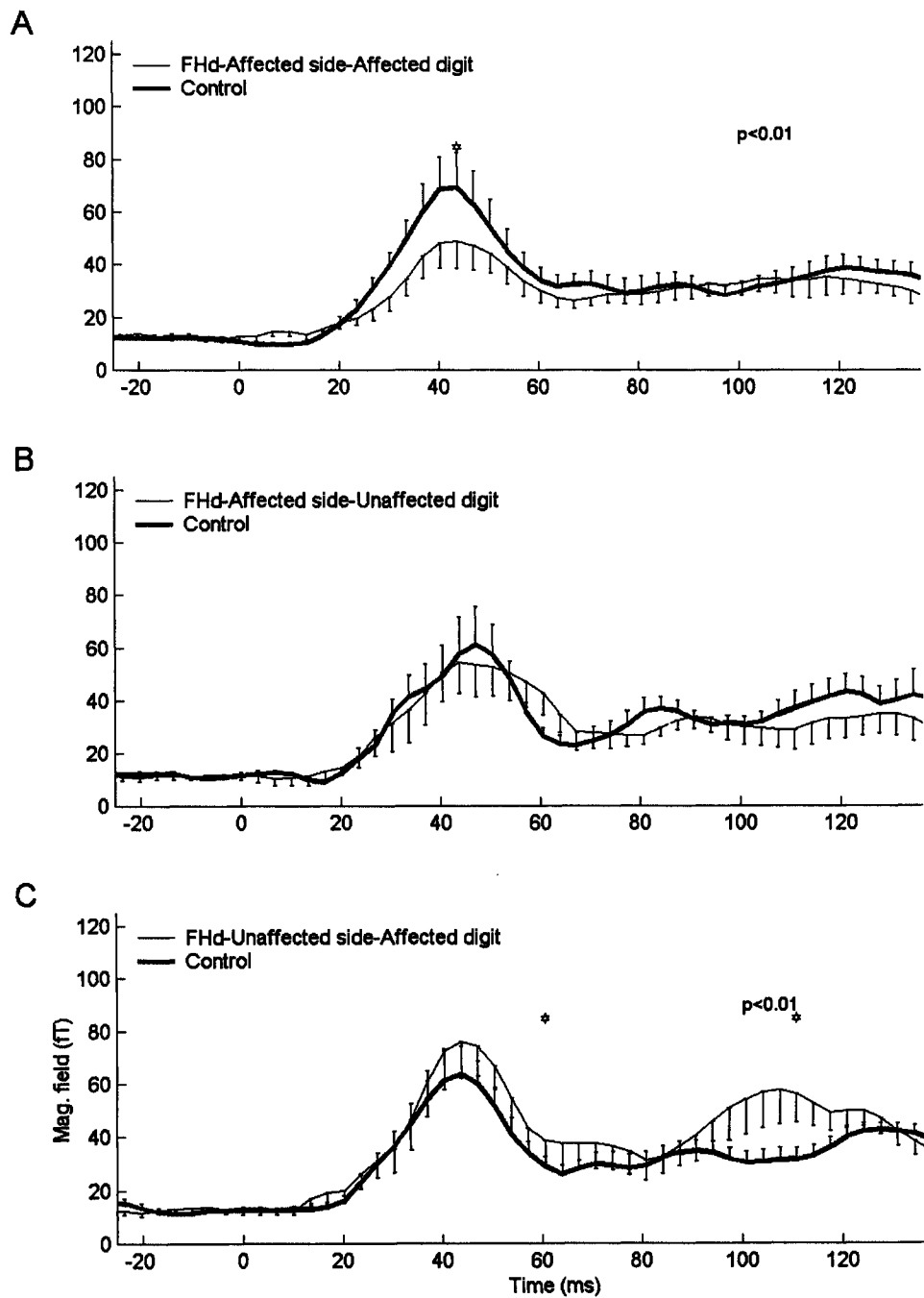
had the first burst of activity at 30 msec (amplitude of  $> 150$  fT) with continued firing at an amplitude of 70 fT even at 120 msec. On the affected side (F), the activity appeared poorly organized with the most activity at 80 msec (60 fT) with continued activity beyond 120 msec.

The distribution of amplitude by latency for the somatosensory evoked field responses for FHD subjects and controls is presented in Fig. 3. When amplitude was integrated across the somatosensory evoked field response time, the amplitude was significantly higher for controls compared with FHD subjects on the affected side, affected digits (A, Fig. 3) but not unaffected digits (B, Fig. 3). On the unaffected side (digits matched to the dystonic digits), however, the amplitude of the somatosensory evoked field response was significantly greater for FHD subjects than for controls (C, Fig. 3).

The scatter plots in Fig. 4 illustrate the distribution of SEF amplitude by latency (by side) for control and FHD subjects. For the FHD subjects, the distribution of amplitude by latency was not linear on the affected side. On scatter plot A, there was a



**Fig. 2:** A visual representation of the differences in amplitude and volume over time for FHd subjects and controls



**Fig. 3:** Somatosensory evoked field responses: amplitude integrated by latency for FHD and control subjects.



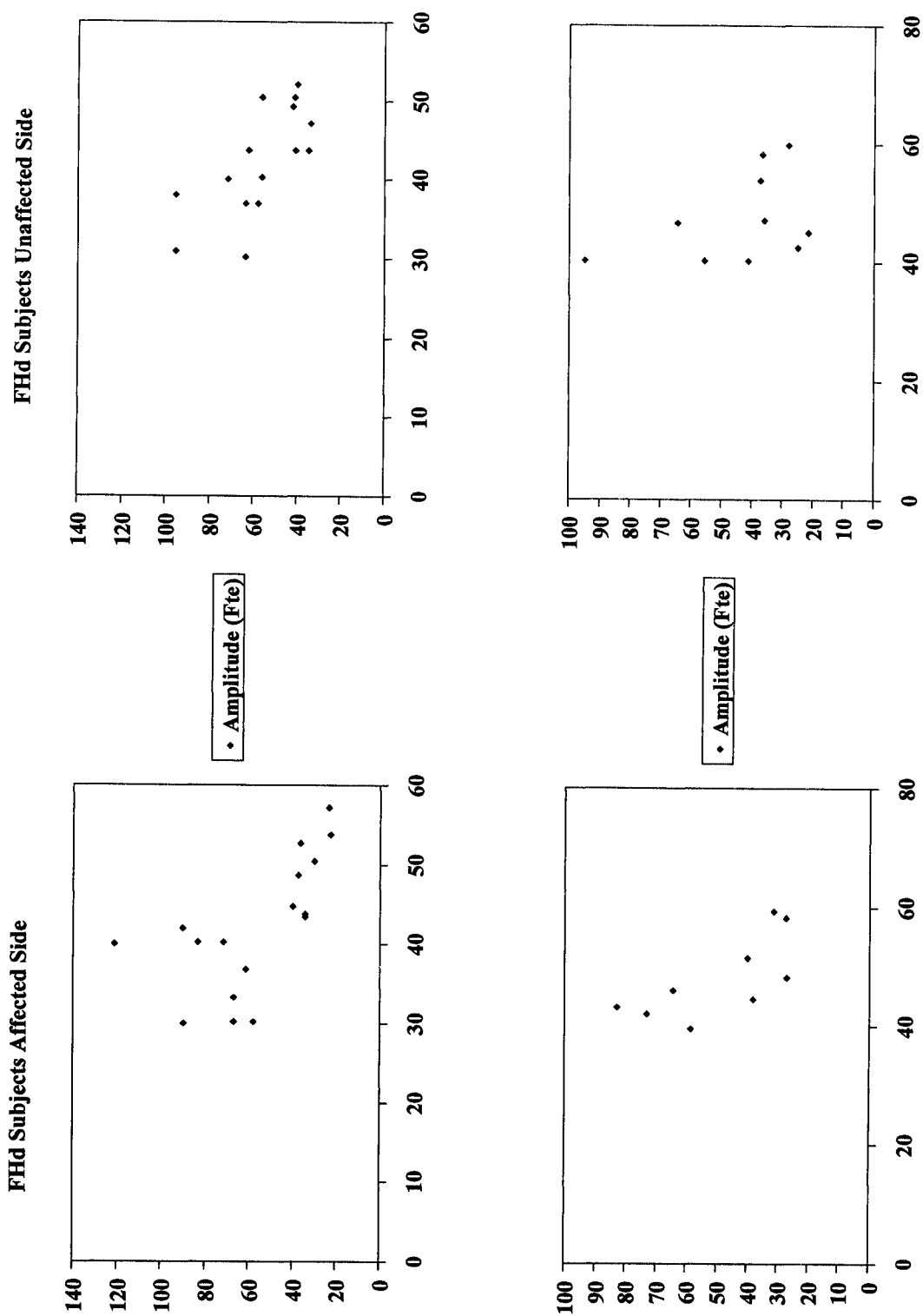
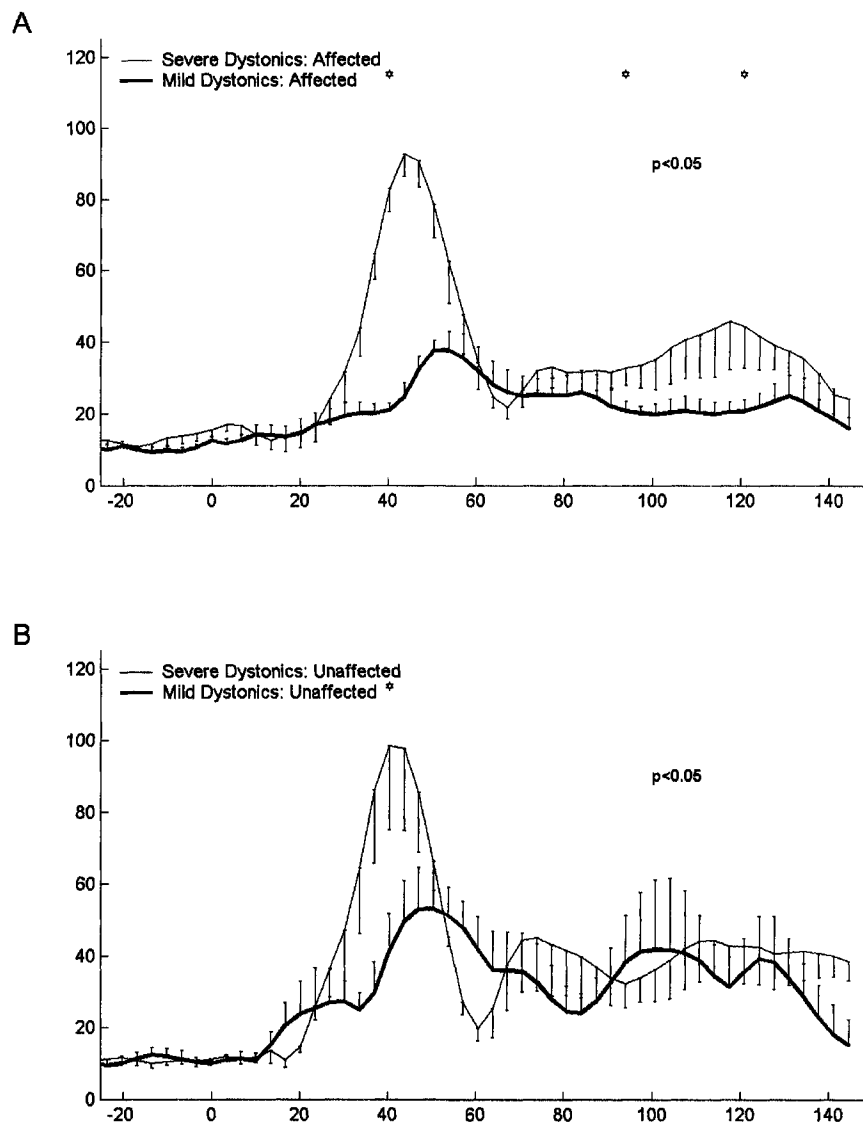


Fig. 4: Distribution of amplitude by latency for the somatosensory evoked field responses: FHd subjects and controls



**Fig. 5** Somatosensory evoked field responses: Amplitude integrated by latency for FHD subjects (severe versus mild dystonia).

bimodal distribution of mean SEF amplitude plotted by mean latency (mean latency ranging from 30 to 60 milliseconds and the mean amplitude ranging from 20 to 119 fT). There was a negative linear trend of amplitude by latency for the digits on the unaffected side for FHD subjects and controls (B, C); as the latency increased, the

amplitude decreased. Figure 5 provides a visual representation of the differences in amplitude integrated by latency for those with severe versus mild dystonia. For subjects with focal hand dystonia, on the affected side, the amplitude of the somatosensory evoked field response was significantly lower for those with *mild dystonia*.

TABLE 7

Somatosensory evoked field responses (SEF): correlation of the ratio of amplitude to latency with severity of FHd and clinical performance criteria

Dependent Variables	Affected Side		Unaffected Side	
	SEF Ratio	Severity of FHd	SEF Ratio	Severity of FHd
Physical Performance	-0.3910*1	-0.3755*2	-0.1071	-0.401*3
Fine Motor Skills	-0.4670 *4	-0.1076	-0.1667	-0.1851
Motor Control Target Task	-0.6116*5	-0.5881*6	-0.7867*7	0.7929*8
Sensory Skills	-0.28271	-0.0062	-0.1077	-0.0402
Pain	-0.19841	-0.3896	-0.2090	-0.0190
	SEF Ratio		Severity of FHd	
Posture/Balance (n=34)	-0.2911		-0.362	
Independence (n=17)	-0.1425		-0.328	

Note: Correlated with severe dystonia coded as "2" and mild dystonia coded as "1"

#### Critical Values

\*1  $z=3.29$ ;  $p<0.0006$  \*3  $z=3.53$ ;  $p<0.0004$  \*5  $z=2.38$ ;  $p<0.0094$  \*7  $z=3.02$ ;  $p<0.0013$   
 \*2  $z=3.31$ ;  $p<0.0005$  \*4  $z=3.67$ ;  $p<0.0004$  \*6  $z=3.47$ ;  $p<0.0004$  \*8  $z=3.13$ ;  $p<0.001$

when compared with subjects with *severe dystonia*. Such a discrepancy in amplitude across latency for those with *mild* compared with those with *severe dystonia* was also measured on the unaffected side.

The digits for the control subjects were orderly sequenced from inferior to superior on the z axis as expected. The digits of FHd subjects were not orderly (see Fig. 6). For example, on the affected side of the FHd subjects, the digits were all represented at the same location.

High, significant correlations ( $0.9029_{\text{affected}}$  and  $0.8477_{\text{unaffected}}$ ;  $p < 0.001$ ) were found between dystonia severity and the ratio of SEF amplitude to latency, respectively (see Table 7). On the affected side, the SEF ratio and dystonia severity were significantly, negatively correlated (moderate to moderately high) with musculoskeletal performance and motor control on the target task; FHd

subjects with *mild dystonia* and those with a low SEF ratio demonstrated higher performance than those with *severe dystonia*. There was also a significantly negative correlation between fine motor skills and the SEF ratio on the affected side; those with a high ratio of SEF amplitude to latency demonstrated greater inaccuracy. Similar to the affected side, on the unaffected side, there was a significant, moderately negative correlation between the severity of dystonia and musculoskeletal performance and a significantly negative correlation between the SEF ratio and motor control at the target task. However, on the unaffected side, there was a significant, positive correlation between the severity of dystonia and motor control on the target task; those with *mild dystonia* had lower scores on the target task than those with *severe dystonia*.

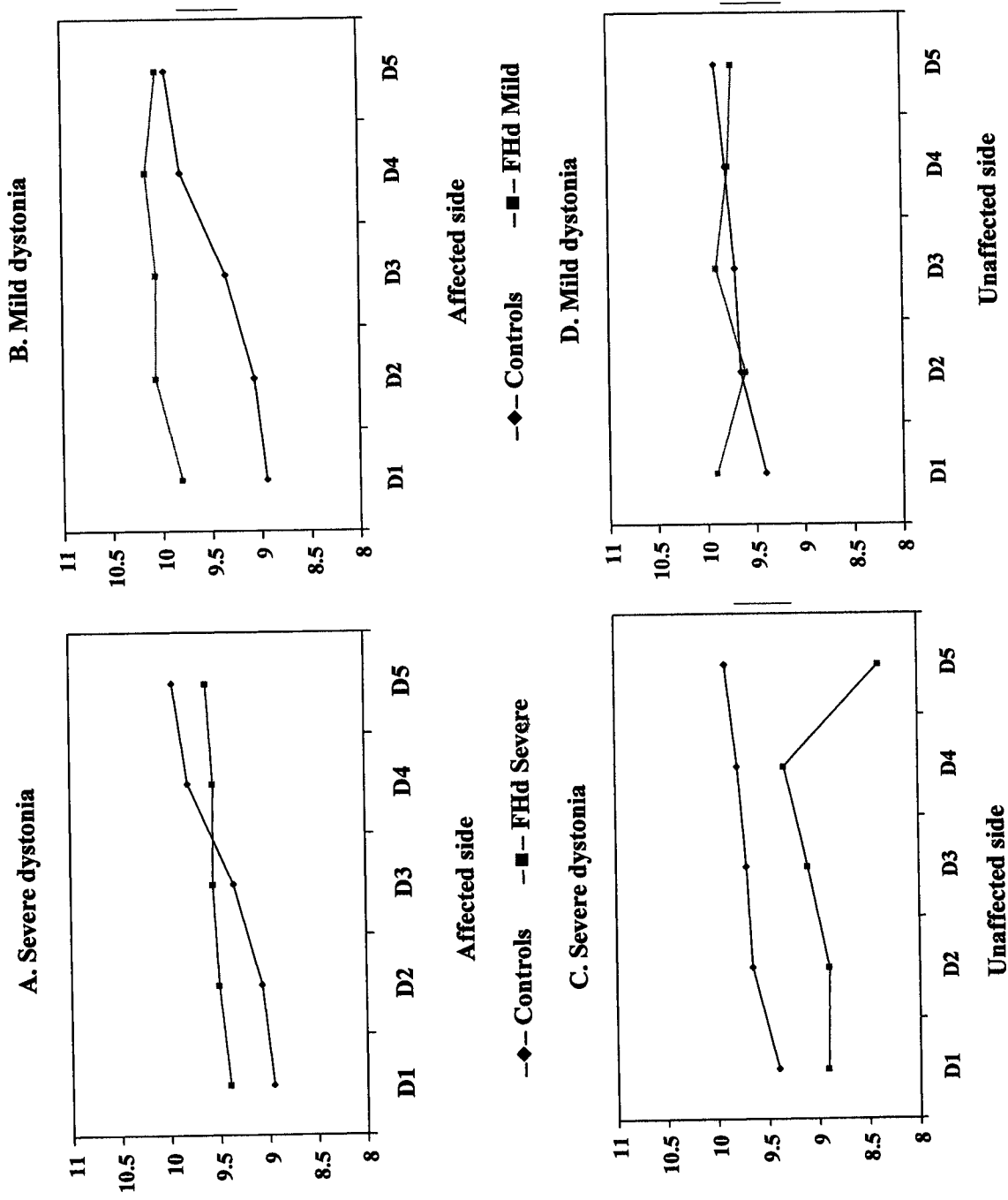


Fig. 6: Sequence of digits on the Z axis: Controls and FHd subjects

## DISCUSSION

The findings from this study contribute new evidence supporting a strong relationship between clinical sensory and motor performance with somatosensory degradation in patients with FHd that distinguishes them from healthy controls and differentiates them by severity of dystonia. The results presented here are consistent with the proposed sensorimotor hypothesis of aberrant learning. The evidence also suggests, however, that FHd subjects do not present as a homogeneous group.

On the affected side, subjects with *severe dystonia* had more musculoskeletal limitations and more impaired task specific motor control compared with those with *mild dystonia*, with the SEP characterized by a short latency, high amplitude, and a reduced area of somatosensory hand representation.

Previous investigators have reported differences in somatosensory evoked responses in FHd subjects (digit clumping, loss of orderly digit sequencing, differences in the size of the area of the somato-sensory hand representation), but no significant difference in mean amplitude (Bara-Jimenez et al., 2000; Byl et al., 1996 a-c; Elbert et al., 1998; Juliano et al., 1991). The findings from the current study indicate that the SEF patterns in those with *severe dystonia* and those with *mild dystonia* are complementary. Thus, when amplitude and latency are averaged across all subjects, the differences are cancelled.

The SEF ratio of amplitude and latency could be viewed as a *neural slew factor*, projecting a linear relation between the clinical severity of FHd and the severity of somatosensory degradation. A high neural slew factor is consistent with a high gain in the sensorimotor feedback loop, whereas a low neural slew factor is consistent with a low gain in the sensorimotor feedback loop (Sanger & Merzenich, 2000). Such feedback errors could

explain the differences noted between the groups in terms of clinical performance. Although previous investigators (Bara-Jimenez et al., 2000; Byl et al., 1996 b-c; Sanger et al., 2000; Tinazzi et al., 1999), reported problems in sensory spatial discrimination in patients with FHd, information on clinical performance and somatosensory structure, as measured by magnetoencephalography, was not reported nor were clinical skills correlated by severity of dystonia. In the current study, subjects with focal dystonia demonstrated compromised clinical sensorimotor performance compared with controls with subjects with *severe dystonia* working faster but making more errors than those with *mild dystonia*.

Restrictions in musculoskeletal structure have been reported in patients with FHd (Wilson et al., 1991; Wilson et al. 1993; Lejinse, 1996). The current study confirms that subjects with FHd have restrictions in musculoskeletal performance when compared with controls, but the finding that subjects with *severe dystonia* had greater limitations in flexibility, strength, and neural tension than those with *mild dystonia* was totally unexpected. Many individuals with tight muscles and joint restrictions develop compensatory movements, but for such movements to resemble dystonia is unusual. Under conditions of stress and repetitive overuse, conceivably musculoskeletal limitations could increase the risk for developing dystonia (Wilson et al., 1991; 1993; Lejinse, 1996). Factors of causality would have to be confirmed by prospective, longitudinal, cohort studies documenting the occupational, physical, sensory, and fine motor characteristics of individuals who perform complex, repetitive hand tasks under stressful environmental or psychological conditions.

In the current study, for subjects with FHd, the fingers were not normally sequenced on the primary sensory cortex on either the affected or the unaffected side, and the size of the hand representation on the affected side was reduced in

comparison with that on the unaffected side. The observation that the hand representation was reduced in those with *severe dystonia* would be consistent with a more serious degradation, including more extensive overlap of receptive fields across the columnar representation of the digits on the cortex. Compared with healthy controls, the size of the area of the hand representation for those with FHd was not significantly different on the affected side; on the unaffected side, however, the area of representation was larger for FHd subjects than for controls. This finding might represent an artifact of the study samples. Compared with control subjects, more FHd subjects were musicians (58.8% versus 17.8%). Musicians reportedly have a larger somatosensory hand representation as a result of complex, repetitive hand use (Elbert et al., 1998). In Elbert's study of violinists, the representation for the left hand (used for complex fingering) was larger than that for the bowing hand. Even though computer keyboard users use their hands intensely, computer keyboarding does not necessitate the same complex movements that are required to play a musical instrument. For example, when playing advanced music on the piano, both hands and multiple digits must play simultaneously and individually with the arms moving concurrently to cover the length of the keyboard. Although some paired digital movements are required on the computer keyboard (e.g. the use of the shift or function key with a letter or number key), most frequently the user depresses one finger at a time. If computer users are applying stress-free hand strategies, then they can depress a single key using the intrinsic muscles (e.g. lumbricals and interossei instead of the long finger flexors) and then simply release the pressure down without requiring a reciprocal digital extension movement. In addition, they can use the mouse at a close distance, moving from the shoulder and elbow to position the mouse and then rotate the forearm to click instead of

using rapid alternating digital movements to click the mouse.

The 'integration times' are primarily dictated by temporal requirements needed to recover from the inhibition that gates movement and dominates post-stimulus excitability. With practice, possibly some individuals can improve performance until they exceed the limits of their integration time. Those who intensively use their hands should be encouraged to achieve precise sensory discrimination, to use intrinsic hand muscles and to avoid excessive overuse of the extrinsic flexors and extensors.

The sensorimotor learning hypothesis is consistent with the principles of neuroplasticity, the finite nature of neural adaptation, and the importance of accurate sensorimotor feedback for fine motor control (Byl et al., 1996; Sanger & Merzenich, 2000). Neuroplasticity is also consistent with the hypothesis that FHd represents a case of aberrant learning. If FHd develops as a consequence of abnormal learning, then patients must first stop the repetition of the abnormal movement and then re-differentiate the somatosensory hand representation by performing attended, progressive, rewarded, sensorimotor behavioral activities (Juliano et al., 1991; Kaas et al., 1983; Merzenich et al., 1982; Merzenich et al., 1996 a-b; Nagarajan et al., 1997; Nakashima et al., 1989).

Our study has several limitations. The data were gathered from a small sample of patients with focal hand dystonia. Two different control groups were used to obtain somatosensory data and clinical performance. The stimulus (air puff) did not represent the minimum threshold stimulus for each individual subject. In the UCSF Biomagnetic Imaging Laboratory, a cutaneous stimulus of 17 to 20 pounds per square inch (psi) was considered an adequate stimulus to indent the skin 400 microns. This stimulus possibly represented a *minimum stimulus* for those whose evoked field response was characterized by a long latency and low amplitude but a *maximum stimulus* for those

responding quickly with a short latency and high amplitude. Preliminary testing of the psi of the stimulus did not confirm this notion, however. An air puff of 15 psi was associated with an increase in amplitude over the 5 and 10 psi stimuli, both for healthy subjects and for patients with FHD, with little differences in the response characteristics at 20 and 25 psi. Minimal differences were found in latency measured between 5 and 25 psi stimuli levels. Thus, it is unlikely that this small force designed to indent the skin 400 microns could explain the consistent differences in somatosensory-evoked responses by severity.

The hypothesis of aberrant sensorimotor learning does not explain why *some* individuals who perform highly skilled, stereotypic, repetitive movements develop FHD and others do not. Issues of 'misuse' versus 'overuse' must be investigated. Possibly, initial, mild abnormal homuncular organization of the digits might result from genetic, congenital, or traumatic conditions. Such differences can be stable, however, until challenged by stress and or highly repetitive, stereotypic movements (Bara-Jimenez et al., 1998; Lejinse, 1999; Byl & Topp, 1998). Teaching individuals how to use their hands in stress-free ways and how to maintain sensitive, precise, accurate sensorimotor processing could serve as an important foundation for the rehabilitation of patients with FHD. More studies are needed to determine if the same strategies could also be used to minimize the risk for developing occupationally related hand dystonia.

### Clinical implications

The findings from this study have significant implications for rehabilitation. This study is the first clearly documenting a correlation between somatosensory degradation and clinical sensory and fine motor performance. It is also the first study noting that clinical performance and somato-sensory function are not homogeneous across all subjects

with focal hand dystonia. These findings could represent aberrant learning within individuals who develop hand dystonia following a stressful history of repetitive overuse of the hand. Thus, theoretically, recovery of fine motor control must be based on the principles of neural adaptation. Logically, the intervention program must be designed to restore the somatosensory organization of the hand including the normalization of sensorimotor feedback. Individuals with severe FHD who demonstrate a high gain in the sensorimotor feedback loop might have to practice behaviors that raise the threshold of sensory excitability until voluntary fine motor outputs are controlled. Subjects with mild FHD demonstrating a low sensorimotor feedback loop gain might have to practice behaviors that lower the threshold of sensory excitability until voluntary fine motor outputs are normalized. All training must be progressive, without causing abnormal, involuntary, motor movements on the target and the related tasks.

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